

## **Temperature behavior of glucose oxidase immobilized into surface-attached stimuli-sensitive copolymer microgel**

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### **Experimental Section**

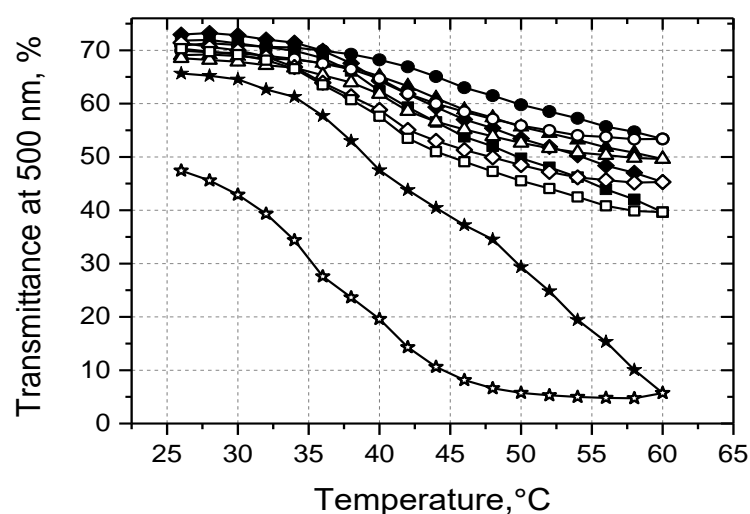
**Materials:** Glucose oxidase (GO) from *Aspergillus niger*, E.C. 1.1.3.4, activity 168100 U/g solid was purchased from Sigma-Aldrich (UK),  $\beta$ -D-glucose was received from ICN Biomedicals, Inc. Tris(hydroxymethyl)aminomethane (TRIS) and its hydrochloride (TRIS-HCl) were obtained from Sigma-Aldrich (Steinheim, Germany). The microgel was synthesized via precipitation polymerization of *N*-isopropylacrylamide (NIPAM) and a cationic comonomer *N*-(3-aminopropyl)methacrylamide (APMA) in the presence of a cross-linker *N,N'*-methylene bisacrylamide<sup>S1</sup> and contains about 16% (mol.) of the cationic comonomer (APMA) units. All other chemicals were of analytical grade and used without further purification. Deionized water (18.2 M $\Omega$  cm) purified with a Milli-Q purification system from Millipore was used as a solvent for preparation of all solutions.

**Turbidimetry;** The transmittance of 0.5 g/L aqueous P(NIPAM-*co*-APMA) microgel solutions prepared in 10 mM TRIS at the specified pH values was measured on a Shimadzu UV-1800 double-beam spectrophotometer (Shimadzu, Japan). The temperature-controlled sample holders were connected to a temperature controller allowing 6 simultaneous measurements. The solutions were heated-cooled with a rate of 0.4°C/min with a step of 2°C and transmittance was scanned with a temperature trend at a fixed wavelength of 500 nm. The cloud points were determined by the lowest point extracted from the derivative of the transmittance versus temperature curve.

**Electrochemical Microgel-Enzyme Constructs:** The screen-printed electrodes (SPEs) were fabricated on poly(vinyl chloride) substrates of 0.2 mm thickness by means of conductive graphite paste (Gwent, UK) screen-printed by a semi-automated Winon machine (model WSC-160B, China) with a 200 mesh screen stencil. Each SPE consisted of a round-shaped working area (2.5 mm diameter), a conductive track (30 mm  $\times$  1.5 mm), and a square extremity (3 mm  $\times$  7 mm) for electrical contact. The SPEs were pre-modified with a peroxide-sensitive layer of manganese dioxide nanoparticles according to procedure described elsewhere<sup>S2</sup>. The SPE/MnO<sub>2</sub> electrodes were stored dry at an ambient temperature until further use. Microgel particles were adsorbed onto SPE/MnO<sub>2</sub> at a temperature of 50 °C via the dip coating method by dipping the electrodes into preheated 1 g/L dispersion of P(NIPAM-*co*-APMA) microgel in 10 mM TRIS of pH 9,5 for 60 min adsorption. After that time, the electrode surface was rinsed with Milli-Q water and was very shortly (for 1–2 s) blown by a stream of air. Directly after this, GO was adsorbed in a similar way from 9 $\times$ 10<sup>-5</sup> M solution in 10 mM TRIS of pH 7 at 20 °C for 40 min, followed by rinsing with Milli-Q water and shortly drying with a stream of air. To prevent the loss of enzymatic activity, the SPE covered by microgel-enzyme films were stored at +4 °C until further use.

**Electrochemical Assay:** Electrochemical experiments were performed in a water-jacket one-compartment electrochemical cell with stirring (volume of 1 mL), using a three-electrode configuration. The SPE/MnO<sub>2</sub>/Microgel/GO constructs were used as the working electrode, while an Ag/AgCl and a platinum wire were served as a reference and a counter electrode,

respectively. A potentiostat IPC Compact (Kronas Ltd., Moscow, Russia) used for electrochemical measurements was interfaced with a PC and electrochemical parameters were controlled by the potentiostat software. The necessary temperature of the water-jacket electrochemical cell was maintained by a thermostat Huber CC-K6 (Huber, Offenburg, Germany). Electrochemical responses were assayed in a 50 mM HEPES/30 mM KCl buffer (pH 7.5, 8.5 or 9) by recording the current arising after the addition of a solution of  $\beta$ -D-glucose with a standard concentration (0.2 mM in the cell). The oxidative current is generated in response to the addition of a substrate ( $\beta$ -D-glucose) solution at an applied potential of +450 mV vs Ag/AgCl. Each electrochemical response was determined as a value of steady-state baseline current change (the difference between an average value of steady-state baseline current before and after the analyte addition).



**Figure S1** Temperature-induced changes of transmittance of a 0.5 g/L P(NIPAM-co-APMA) microgel dispersion in 10 mM TRIS at different pH values: pH 7.5,  $T_{CP}$ = 44°C,  $\alpha$  = 0.89 (circles); pH 8,  $T_{CP}$ = 43°C,  $\alpha$  = 0.84 (triangles); pH 8.5,  $T_{CP}$ = 40°C,  $\alpha$  = 0.76 (diamonds); pH 9,  $T_{CP}$ = 39°C,  $\alpha$  = 0.62 (squares); pH 9.5,  $T_{CP}$ = 38°C,  $\alpha$ =0.45 (stars). Solid and open symbols correspond to heating and cooling, respectively. The cloud point ( $T_{CP}$ ) for each pH was determined as a minimum of the derivative of the heating part of the corresponding transmittance-temperature curve. The values of the degree of protonation ( $\alpha$ ) were extracted from the potentiometric titration data <sup>S1</sup>.

## References

- S1. L. V. Sigolaeva, D. V. Pergushov, M. Oelmann, S. Schwarz, M. Brugnioni, I. N. Kurochkin, F. A. Plamper, A. Fery and W. Richtering, *Polymers*, 2018, **10**, 791.  
 S2. L. V. Sigolaeva, U. Günther, D. V. Pergushov, S. Yu. Gladyr, I. N. Kurochkin and F. H. Schacher, *Macromol. Biosci.*, 2014, **14**, 1039.