

Poly(ϵ -caprolactone-co- ω -pentadecalactone) electrospun fibers

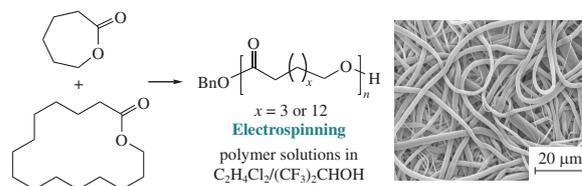
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DOI: 10.1016/j.mencom.2020.01.015

Electrospun fibers with appropriate morphology have been prepared from ω -pentadecalactone/ ϵ -caprolactone random copolymers when polymer solutions in 1,2-dichloroethane/hexafluoroisopropanol media were used for molding.



Keywords: biodegradable polymers, ϵ -caprolactone, copolymerization, electrospinning, fiber, ω -pentadecalactone, ring-opening polymerization.

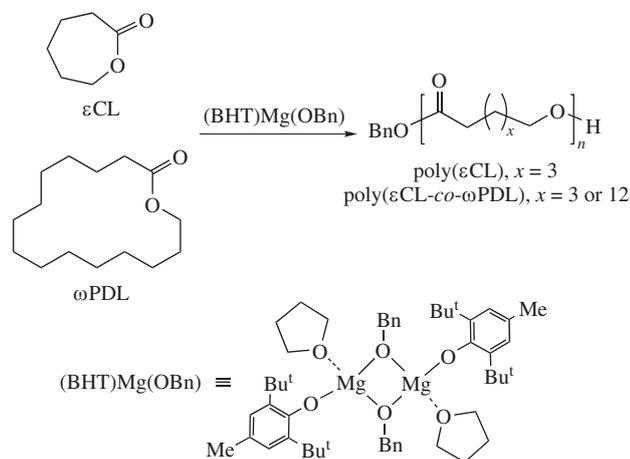
Ring-opening polymerization (ROP) of knowingly non-toxic monomers is widely used in the synthesis of prospective polymers.^{1–4} Among lactones, ω -pentadecalactone (ω PDL, pentadecanolide, a famous musk-odoured fragrance) draws attention due to the presence of extended linear hydrocarbon chains. This allows one to consider ω PDL-based polymers (Scheme 1) as a kind of the bridge between polyolefins and polyesters. Due to promising mechanical characteristics, relatively slow resorbability, and applicability of wet-spinning,^{5,6} ω PDL polymers represent prospective materials for industrial and biomedical use.^{7–14}

Synthesis of ω PDL polymers has been extensively described. Homopolymerization of ω PDL was carried out in the presence of organocatalysts,^{15,16} metal complexes^{17–22} and enzymes.^{23,24} Block copolymers of ω PDL with L-lactide²⁵ and lactones^{25,26} were also prepared, however random ω PDL copolymers look more promising due to homogeneity of physical characteristics. To date, random copolymers of ω PDL with different cyclic esters have been synthesized and characterized.^{27–31} Copolymers with

ϵ CL are of particular interest because poly(ϵ CL)/poly(ω PDL) materials demonstrate shape memory effect.^{32–35}

Electrospun (ES) fibers are highly attractive for biomedical purposes due to specific morphology resembling extracellular matrix and providing the possibility of using the ES materials in surgery, tissue and neural engineering. Up to now, ES fibers were prepared from ω PDL homopolymers⁵ and copolymers of ω PDL with L-lactide.³⁶ Poly(ω PDL) ES scaffolds are not cytotoxic and support cell proliferation.⁵ Some problems remain unsolved in morphology and mechanical properties of ES fibers based on ω PDL.^{5,36} These problems are caused by heterogeneity of the ROP products, gel formation and uneven evaporation of the solvents.⁵

Here, we report on the preparation of ES fibers based on random ω PDL/ ϵ CL copolymers, and comparison of the morphology and mechanical characteristics of these materials with ES fibers based on poly(ω PDL). In the synthesis of homo- and copolymers, we used highly active and non-toxic BHT-Mg catalyst^{17,37} (see



Scheme 1

Table 1 Polymerization experiments.

Run	ω PDL ^a	ϵ CL ^a	$M_n \times 10^3$ theory	$M_n \times 10^3$ (NMR) ^b	$M_n \times 10^3$ (SEC) ^c	\bar{D}_M (SEC) ^c	DSC peak / °C	
							1 st heat	2 nd heat
1	100	0	24.1	27.8	57.6	2.05	99.27	96.31
2	150	0	36.2	36.8	76.5	2.29	98.91	97.64
3	200	0	48.2	43.6	96.4	2.12	99.81	98.89
4	300	0	72.2	79.4	117.1	2.26	99.68	99.22
5	150	50	41.9	37.4	83.8	2.18	87.26	86.09
6	100	100	35.6	29.7	74.8	2.19	81.06	79.24

^a Monomer/[Mg] molar ratio. ^b Calculated by the formula M_n (NMR) = 108.14 + P_n ($x M_{\omega\text{PDL}} + y M_{\epsilon\text{CL}}$), where 108.14 is MW of BnOH, P_n is degree of polymerization determined as a ratio of integrals in ¹H NMR spectra of the signals of polymer OCH₂ fragments and CH₂OH end-groups, x and y are normalized molar fractions of ω PDL and ϵ CL, respectively, for poly(ω PDL) $x = 1$, for poly(ϵ CL) $y = 1$, for poly(ϵ CL-co- ω PDL) $x + y = 1$. ^c Determined by SEC in 1,2,4-trichlorobenzene at 50 °C vs. polystyrene standards.

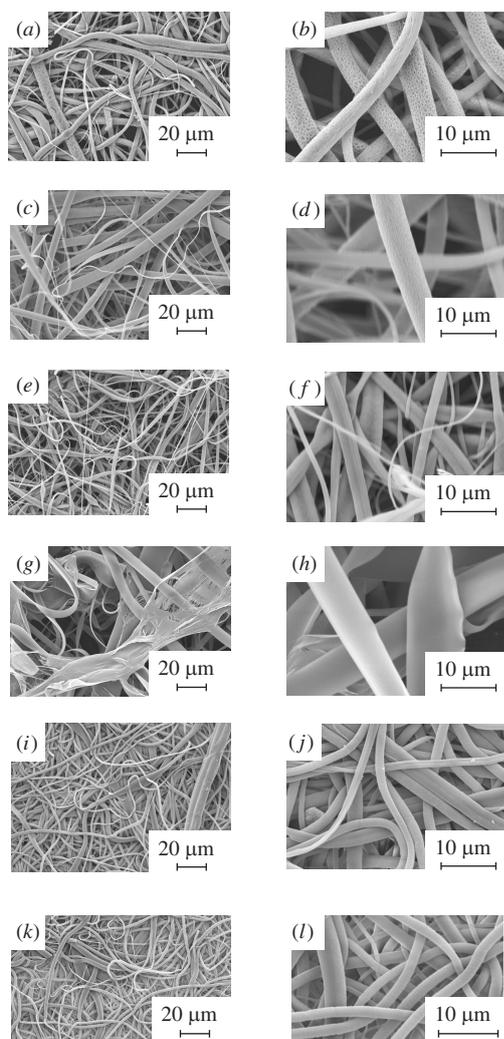


Figure 1 SEM images of electrospun fibers molded from poly(ϵ CL-*co*- ω PDL) [Table S1, runs: (a,b) – 1, (c,d) – 2, (e,f) – 3, (g,h) – 4, (i,j) – 5, (k,l) – 6, see Online Supplementary Materials].

Scheme 1). Polymerization experiments were conducted at 100 °C in molten comonomer mixtures[†] (Table 1). The polymers obtained have slightly broadened \mathcal{D}_M due to diversification of the catalyst *via* the formation of more active mononuclear catalytic species in the course of reaction.^{17,37,38} A noticeable difference in molecular weight (MW) values determined by NMR and by SEC could be attributed to the need to take into account the correction factor for polyester analysis using the PS standard; for ϵ CL, the value of this factor is 0.56. The presence of single sharp peaks in DSC of poly(ϵ CL-*co*- ω PDL) samples confirmed statistical nature of copolymers. Depending on the comonomer ratios, these peaks were shifted towards lower temperatures relative to DSC peak of poly(ω PDL) samples (see Table 1).

As was found earlier, CHCl_3 is the only good solvent for poly(ω PDL), however nanofibers obtained from solutions in pure CHCl_3 exhibit ‘bead’ defects.⁵ We optimized the parameters of ES laboratory device, and studied electrospinning of 10 wt% solutions of poly(ϵ CL-*co*- ω PDL) (comonomer ratio 150:50, see Table 1, run 5) in various media (for details, see Table S1 in the Online Supplementary Materials). When $\text{CHCl}_3/\text{EtOH}$ was used, the fibers 1–4 μm in diameter with highly porous surface were obtained [Figure 1(a),(b)]. These defects almost disappeared when

[†] Visually, under these conditions polymerization finished after 5–10 min, the reaction mixtures were kept for additional 40 min. For experimental details and NMR spectra, see Online Supplementary Materials.

Table 2 Mechanical properties of electrospun mats obtained.

Run	ω PDL/ ϵ CL ^a	$M_n \times 10^3$ (NMR)	E^b/MPa	σ_p^c/MPa	ϵ_p^d (%)
1	150/50	37.4	11 ± 2	5.9 ± 1.0	336 ± 20
2	100/100	29.7	8 ± 2	4.2 ± 0.8	305 ± 18
3	100/0	27.8	10 ± 3	2.4 ± 0.5	175 ± 14
4	150/0	36.2	11 ± 2	5.1 ± 1.1	344 ± 21

^a Comonomer molar ratio relative to mole of Mg. ^b Young’s modulus. ^c Tensile strength. ^d Elongation at break.

CHCl_3 was replaced by higher boiling point solvent, *e.g.*, with 1,2-dichloroethane [Figure 1(c),(d)]. However, both samples included significant amounts of ultra-thin threads. The addition of minimal amount of formic acid resulted in lowering the fiber diameter to 0.5–3 μm [Figure 1(e),(f)], but some ribbon-like structures were detected. We got the idea to use hexafluoroisopropanol (HFIP) instead of EtOH from the positive impact of the presence of acid. Electrospinning of polymer solution in HFIP [Figure 1(g),(h)] has yielded highly porous mats containing flat polymeric segments. Nevertheless, when 1,2-dichloroethane/HFIP mixture was used, we obtained fibers with desired homogeneous morphology, the main part of the fibers had a diameter of 2–4 μm without ultra-thin threads and ribbons. The optimal $\text{C}_2\text{H}_4\text{Cl}_2/\text{HFIP}$ ratio was found to be 4:1 [Figure 1(i)–(l)]. We also studied electrospinning of poly(ω PDL) samples with different MW (see Table S1, runs 7–10) and found that for 10 wt% polymer solutions the optimum P_n value for the formation of homogeneous fibers was ~200 (Figure S5). The results of the mechanical test (Table 2)[‡] of the fibrous mats obtained in ES (see Table S1, runs 5–8) demonstrate close characteristics for poly(ω PDL) and poly(ϵ CL-*co*- ω PDL) ES materials.

In summary, we managed to get electrospun mats from poly(ω PDL) and random poly(ϵ CL-*co*- ω PDL) with uniform morphology. These results were achieved by the application of 1,2-dichloroethane/HFIP as the solvent. Poly(ω PDL) ES fibers are close to poly(ϵ CL-*co*- ω PDL)-based fibers by morphology and mechanical characteristics. In this way, copolymers of ω PDL with lower MW lactones hold promise in the development of fibrous materials with regulated hydrophilicity. The studies of biocompatibility and biodegradation of new fibrous poly(ϵ CL-*co*- ω PDL)-based materials are ongoing in our laboratory.

This work was supported by the Russian Science Foundation (grant no. 16-13-10344-P, in part of polymer synthesis and formation) and was carried out within the State Program of TIPS RAS (in part of polymer analysis).

Online Supplementary Materials

Supplementary data associated with this article can be found in the online version at doi: 10.1016/j.mencom.2020.01.015.

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[‡] Mechanical tests were carried out on a TiraTest-2200 tensile machine (movement speed: 5 mm min⁻¹, the sample geometry was 10 × 3 × 0.03 mm).

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Received: 12th July 2019; Com. 19/5984